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(54) A Carcinostatic Agent Prepared From Microspheres, and the Manufacturing Method Thereof.

(21) Patent Application

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Specifications

1. Name of the Invention

A Carcinostatic Agent Prepared From Microspheres, and the Manufacturing Method Thereof.

2. Scope of the Patent Claim

- 1. A carcinostatic agent prepared from microspheres formed from 1-n-hexylcarbamoyl-5-fluorouracil and polylactic acid, or from the uniform compound with its copolymer.
- 2. A method of manufacturing a carcinostatic agent prepared from microspheres formed from 1-n-hexylcarbamoyl-5-fluorouracil and polylactic acid or from the uniform compound with its copolymer, attained by stirring 1-n-hexylcarbamoyl-5-fluorouracil, dissolved in methylene chloride, and polylactic acid or its copolymer solution into an aqueous gelatin solution preserved at pH values between $3 \sim 6$.

3. Detailed Description of the Invention

This invention is concerned with a controlled-release carcinostatic agent prepared by formulating 1-n-hexylcarbamoyl-5-fluorouracil into microspheres, and the manufacturing method thereof.

The "carcinostatic agent prepared from microspheres" of this invention is a carcinostatic agent structured from microspheres possessing granular particles with grain diameter $10\sim300~\mu$, which are formed by uniformly solidifying a solution of polylactic acid (or its polymer) and 1-n-hexylcarbamoyl-5-fluorouracil.

1-n-hexylcarbamoyl-5-fluorouracil (abbreviated HCFU hereafter) is a masking compound of the carcinostatic agent 5-fluorouracil (abbreviated 5-FU hereafter). 5-FU is known among antimetabolite carcinostatic agents as an agent with excellent medicinal efficacy, but it has the following shortcomings: it has a short metabolic half-life, it is highly toxic, and induces impediment of the digestive organs, in particular.

In order to improve on these shortcomings, HCFU was recently developed as one element for use in an oral carcinostatic agent. HCFU is already considered an exceptional carcinostatic agent with regard to carcinostatic activity, blood concentration duration, and hypotoxicity, but if it is administered continually over a long period of time, the complete suppression of side effects cannot be guaranteed.

Active research is performed with regard to dosage methods and medicine shape, in which a carcinostatic agent, which can be administered locally, is administered as a carcinostatic treatment to the cancer-affected region alone and prevents side effects to the regions of normal cells, while simultaneously using an exipient such as resin and considering the durability of the medicine.

As a known method of so-called "controlled-release local dosage," which supplies the effective ingredient quantity of carcinostatic agents continually over an extended period of time to the cancer-affected region alone, there is, for example, a method in which a carcinostatic agent is inserted into a capsule or formed into a pill-shaped material and buried within the cancer-affected region. There is also a method in which agents are formed into microcapsules with a polymerized film through a coacervation of carcinostatic agents, or the polymer and the agent are dissolved together using the same solvent and uniformly solidified at the molecular level, then separated and cast into a microsphere agent. This agent is then injected into a muscle or blood vessel of the affected region, creates an embolus in the capillary vessels of the affected region with these capsules or spheres, and infiltrates only the blood vessel obstructed by the embolus.

In cases in which carcinostatic agents that are prepared with microcapsules or microspheres are used as the embolus for the blood vessel of the affected region, materials with a uniform grain diameter under the vicinity of 200 μ are normally required. Furthermore, the microspheres must have a prescribed controlled-release effect; therefore, microcapsules that have been capsulized outside a prescribed grain diameter have a uniform film, and it is necessary that materials that have been formed into microspheres be prepared such that they have a homogeneous mixture. An organism-resorptive macromolecular material is ideal for the polymer that forms the base for the film or mixture used as the excipient for the microspheres, but ethyl cellulose or polyvinyl alcohol are normally used in the preparation of microspheres. Polyglycolic acid and polylactic acid are organism-resorptive macromolecular materials, but they have such physical limitations as: the melting temperature and viscosity of polyglycolic acid are high, and the glass transposition temperature of polylactic acid is low, while its viscosity is high. Therefore, it is considered difficult to obtain uniform microspheres with these organism-resorptive macromolecular materials.

Therefore, there have been very few cases in which polyglycolic acid (or its copolymer) or polylactic acid (or its copolymer) were actually used to create microcapsules and microspheres (microspheres are usually called microprills), but it is documented in the patent release report S54-55717 that polylactic acid was applied under extremely low temperature conditions $(-40 \sim -100^{\circ}\text{C})$.

In the public report mentioned above, when microcapsules are manufactured at such low temperatures as $-40 \sim -100$ °C, the capsulized core materials are insoluble like toluene. In the case in which polylactic acid uses a solvent with a low freezing point and isolates the microscopic grains of the core material to manufacture microspheres, both the polymer and the micro-granulated agent core are dissolved using a solvent mixture of toluene and chloroform. Microspheres are manufactured by adding a phase separating agent such as polyvalent alcohol, which is a non-solvent to counterbalance the solvent, to these low-temperature solutions, and then separating capsule grains or sediment grains.

In the case of carcinostatic agents formulated from microspheres, the shape of the finely ground agent grains is not normally uniform, so it is difficult to obtain a uniform film in microcapsulation. Therefore, although it is said that microspheres are suitable with regard to their prescribed controlled-release effect, in order to formulate these grains into microspheres, it is necessary to completely dissolve the medicine. However, as in the report described above, there are very few solvents that will dissolve both polylactic acid (or its copolymer) and a known carcinostatic agent, and it can therefore be concluded that, in this report, the core grains of the agent needed to be micro-granulated.

In the midst of earnestly investigating microspheres within an HCFU microsphere agent, the authors of this invention discovered the unexpected result that HCFU and polylactic acid (or its copolymer) are highly mutually soluble. The inventors discovered that an agent that is prepared from pellet-shaped microspheres, which are created by uniformly combining these materials through solidification, has powerful controlled-release efficacy as a carcinostatic agent.

Furthermore, the inventors learned that very-low temperature implementation and preprocessing for microgranulation are unnecessary, and that by combining a particular solvent with a particular phase-separating agent, there is absolutely no cohesion among like microspheres. Finally, the inventors discovered that uniform HCFU microspheres with an average grain diameter of less than 200 μ could be obtained, which are ideal for cases in which the above materials are used with an embolus present in the blood vessels of a cancer-affected region.

This invention provides an HCFU carcinostatic agent prepared from microspheres formed from 1-n-hexylcarbamoyl-5-fluorouracil and polylactic acid, or from the uniform compound with its copolymer, and a manufacturing method thereof.

The polylactic acid (or its copolymer) used in this invention is a copolymer of poly-D, L-lactic acid, and glycolic acid with over 50% lactic acid content, and a macromolecule that has a polylactic acid with a characteristic viscosity between $0.5 \sim 1.5$ (measured at 0.5% density within a mixed solution of 10-weight phenol and 7-weight trichloric phenol at 30 ± 0.1 °C) would be ideal.

The microspheres of this invention, which are formulated from polylactic acid and HCFU, can be manufactured in the manner described below.

At room temperature, add a type of polylactic acid and an amount of granulated HCFU totaling less than 40% of the weight of the polylactic acid (ideally around $1\sim10\%$) to a solution of methylene chloride. It is best to use polylactic acid with a diluted concentration between $1\sim10\%$ of that of the methylene chloride. Prepare separately an aqueous gelatin solution with a pH value regulated between $3.0\sim6.0$ (ideally between $4.0\sim5.0$) by diluting $0.3\sim0.5\%$ of the aqueous gelatin solution with dilute hydrochloric acid. With an aqueous gelatin solution with a pH value greater than 6.0, the HCFU will undergo hydrolysis when the methylene chloride solution is added, so this is not desirable. Also, uniform microspheres cannot be obtained with a pH value less than 3.0. Stir methylene chloride, in which the HCFU and a type of polylactic acid are dissolved, into this acidic aqueous gelatin solution, and by slowly increasing the temperature from $30\sim60^{\circ}\text{C}$, methylene chloride from within the emulsified solution will foam in a micelle shape and evaporate. By increasing the temperature over several hours the methylene chloride will completely evaporate, so then remove and isolate the upper stratum of condensation, and wash away the gelatin residue with warm water with a pH value between $4\sim5$. By then performing vacuum dehydration, white microspheres with grain diameter between $10\sim300~\mu$ can be obtained, and there will never be any methylene chloride residue on the spheres.

Microsphere carcinostatic agents containing HCFU that are obtained in this way are a grain-shaped uniform mixture of a biopolymer-based agent of a type of polylactic acid and HCFU, and these carcinostatic agents possess prescribed controlled-release properties.

Below we demonstrate an example of execution.

Examples of Embodiment

After stirring and dissolving 1.8 g of poly-DL lactic acid (measured at $30\pm0.1^{\circ}\text{C}$ with 0.5% density within a mixed solution of phenol and trichloric phenol with a 10/7 weight ratio) with a characteristic viscosity value $\eta=0.63$ into 40 g of methylene chloride, we added 0.2 g of 1-n-hexylcarbamoyl-5-fluorouracil (HCFU) [made by Mitsui East Pressure Chemistry, Inc.; product name: Miflor], completely solubilized the solution, and obtained a uniform, transparent solution.

Separately, we then added 2 g of acid treatment gelatin [made by Kyujo Chemistry, Inc., jelly strength: 250] to 198 g of water, dissolved the solution by increasing the temperature to 50°C, and produced 1% aqueous solution. After cooling the solution to air temperature, we adjusted the pH level to 4.5 with dilute hydrochloric acid.

We moved this aqueous gelatin solution into a 500 ml beaker, added the above-mentioned methylene chloride solution, and after stirring and emulsifying the solution for 5 minutes using a 5 cm churning shuttlecock at 300 rpm, we evaporated the methylene chloride while gradually heating from the outside. The interior temperature reached 50° C after approximately 30 minutes, and we then confirmed that the odor of methylene chloride had completely disappeared, and ended the microsphere-creating process. We removed the faint condensation on the upper stratum, and after wiping and flushing the system with warm water with a pH value of 4.5, we air-dried the solution at 50° C and obtained a 1.6 g spherical, white microsphere with grain diameter between $30 \sim 200~\mu$.

The chemical element analysis values of this microsphere were as expressed in the chart below, and it uniformly contained 9.3% HCFU. Also, the results of chlorine analysis showed absolutely no signs of methylene chloride content.

Test Example

After dissolving a fine powder of HCFU in physiological saline with a pH value of 6 and leaving it for one day and night, we measured the ultraviolet spectrum of this saline broken down by the eluted HCFU. We confirmed that the absorbance and density were directly proportional, and created the following calibrating curve.

1.	7	0.135
2.	14	0.28
3.	21	0.426
4.	28	0.551
5.	35	0.686

Using this, we inserted 100 mg of the microsphere, which was obtained in the example of execution and contained 9.3% HCFU, into 50 ml of physiological saline. Immediately after directly sampling $1 \sim 3$ ml each day of measurement, we measured the UV spectrum and obtained the results of the following chart.

# Days	l	4	6	7	8	11	15	20
Eluted 5-FU (ppm)	7.5	19	22	24	26	31	36	38
Elution Ratio (%)	4	10	12	13	14	17	19	20

From this chart, it was confirmed that the HCFU carcinostatic agent, which was formulated from microspheres obtained from the example of execution, had a long-term controlled-release effect.

Patent applicant:

Mitsui East Pressure Chemistry, Inc.

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函微小球に製剤された制ガン剤及びその製造方法

②)特

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明 細 群

1. 発明の名称

微小球に製剤された側ガン剤及びその製造方法。

- 2. 特許請求の範囲
 - (1) 1-n-ヘギシルカルバモイル-5-フルオロウラシルとポリ乳酸またはその共産合体の均質混合物よりなる微小球に製剤された側ガン剤。
 - (2) 塩化メチレン化粉解された 1 n ヘキシルカルバモイル 5 フルオロウラシルとポリ乳酸またはその共重合体務液を P H 3 ~ 6 化維持されたゼラチン水溶液 中に攪拌下添加で得られる、 1 n ヘキシルカルバモイルー 5 フルオロウラシルとポリ乳酸またはその共重合体よりなる微小球に製剤された制ガン剤の製造方法。
- 3. 発明の詳細な説明

水発明は、1-n-ヘキシルカルバモイル-

5 - フルオロウラシルを微小球に製削した徐放性制ガン削及びその製造方法に関する。

本発明で「微小球に製剤された側ガン剤」と

は、ポリ乳酸またはその共重合体と1-n-ヘキシルカルバモイル-5-フルオロウラシルが均質に固裕化されていて顆粒状となつた粒径
10~300μを有するマイクロスフェア(micro sphare) 構造の酸小球側ガン剤である。
1-n-ヘキシルカルバモイル-5-フルオロウラシル(以下、HCFUと略する。)は、側ガン剤5-フルオロウラシル(以下、5-FUと略する。)な中でも対して知られているが、代謝半減切使れた薬剤として知られているが、代謝半減

このような欠点を改善するため、経口側ガン 削用の一つとして最近HCFUが開発された。 HCFUは側ガン活性、血中機度特続時間、低 舞性などの点ですぐれた側ガン剤としてすでに

管障害をおとす欠点がある。

定評があるが、やはり、 経口制ガン削として大 量投与、長期連続投与すれば消化器系の副作用 の抑制は必ずしもゼロとは云えない。

一方、最近の側ガン療法として局部投与可能な制力ン剤をガン患部周辺のみに投業して正常細胞個所への創作用を防止し、同時に樹脂などの賦形剤を用いて要効の持続性を考慮した投薬方法や、薬剤形態の研究も確んにおこなわれている...

ラス転位温度が低く、避離粘度が高いなどの物性上の側約があり、これらの生体吸収性高分子 材料では均一な微小球は得られがたいとされている。

このためマイクロカプセルまたはマイクロスフェア(通常マイクロスフェアをマイクロフリルとも云う。)にポリグリコール酸またはその共産合物を用いた例は極めて少ないが、特開昭 5 4 ー5 5 7 1 7 公報には、ポリ乳酸を用いてー4 0

~-100℃の射低温条件下で実施されている 記載がある。

前記公報では、一10~一100℃の低温で、マイクロカブセルを製造する場合はトルエンなどのようにカブセル化されるコア材料は不溶性であり、ポリ乳酸は溶解する薬結点の低い溶解を川いてコア材料微粒子を分散させ、またマイクロスフェアを製造する場合は、トルエンにクロホルムなどを混合した溶媒を用いて重合物及び微粒化した薬剤コアーの両者を溶かし、こ

内内ないしは血管内に注入し、局部周辺の毛細血管内に核カプセルまたはスフェアで塞栓して 開栓された局部血管のみに薬剤の凝出を利用する方法などが挙げられる。

マイクロカプセルまたはマイクロスフェアな どの微小球に製剤された制ガン剤を局部周辺血 管の塞栓として用いる場合は、通常粒径200 μ程度以下の均一な枚径を有するものが要求さ れる。また、これらの微小球は一定の徐放効果 のあるものが必要であり、そのためには一定粒 径の外にマイクロカプセルされたものは均一な 被膜を有しており、マイクロスフェアされたも のは均質を混合を有するよう製剤する必要があ る。また微小球に賦形するための被膜や混合薬 削となる重合物は、生体吸収性の高分子材料が 好ましいが、微小球の製剤には通常、エチルセ ルローズ、ポリビニールアルコールなどが使用 されている。ポリグリコール酸、ポリ乳酸類は 生体吸収性高分子であるが、ポリグリコール酸 は溶融温度及び溶融粘度が高く、ポリ乳酸はガ

れらの低温溶液中に溶媒に対して非溶媒である多価アルコールなどの相分離剤を添加してカンセル粒子または沈澱物粒子を析出させて製造されている。

通常、微小球に製剤された制ガン剤の場合、 微粉末化された薬剤粒子の形状が均一ではない ので、マイクロカプセル化では均一な被膜がイク ないので、薬剤の一定徐放外果の点ではマイクロ ないので、薬剤の上定徐放外果の点が、マイクロ のフェアがよいと云われているがおさせイクロ スフェアにするためには剤を完裕のように超低 がある。しかしながら、前配公報のように超低 温では、ボリ乳酸またはその共重合体は非常な少 のは、前配公報はそのため、薬剤などののと思われる必要があつたものと思われる。

本発明者らは、HCFU像小球製剤の中でマイクロスフェアを鋭意検討している中に、驚くべきことにHCFUはポリ乳酸またはその共重合体とは相溶性がよく、両者は問辞化により均

質に混合され、数小球顆粒状のマイクロスフェアに製剤されたものは側ガン剤として徐放効果の大きいことがわかつた。しかも、超低温での実施やHCFリの超微粒化の前処理もなどに、特定が吸と特定の相分離剤を組み合せるととにより、マイクロスフェアの過ぎの影響という。 特にガン発生局部周辺血管内に霧栓状下の均とより、はのでは、 は、サイクロスフェアが得られることもわかつた。

本発明は、1-n-ヘキシルカルバモイルー5-フルオロウラシルとボリ乳酸またはその共産合体の均質混合物よりなるマイクロスフェア
微小球に製剤されたHCFU制ガン剤及びその
製造方法を提供するものである。

水発明に用いるポリ乳酸またはその共重合体は、ポリーD、 L-乳酸、乳酸 5 0 多以上のグリコール酸との共正合物であり、固有粘度 0.5~1.5 を(フェノール1 0 重量部とトリクロロフェノール7重低部の混合溶媒中3 0 ± 0.1 C

の塩化メチレンは起泡しながら蒸発する。数時間加温すれば、塩化メチレンは完全に蒸発除去されるので、上層の凝集物を除き、炉過分離し、PH 4~5の温水で残留するセラチンを洗浄除去して、再空を燥すると、10~300μの粒径の白色のマイクロスフェアが得られ、マイクロスフェア中には塩化メチレンは全く残留するととはない。

このようにして得られたHCFU含有の微小球側ガン剤は、ボリ乳酸類の生体高分子粘剤とHCFUが均質に混合された顆粒状になつており、一定の徐放性を有する。

以下、災施例を示す。

寒施例

問有粘度値[n]= 0.63 を行するポリDL乳酸[フェノール/トリクロロフェノール=10/7(重量比)の混合密剤中30℃に於ける濃度 0.5 多で測定〕1.8 タを塩化メチレン409に攪拌しながら溶解したのち、1-

の濃度 0.5 % で測定)有する為分子のものが好ましい。

本発明のポリ乳酸類とHCFUよりなるマイクロスフェアは以下のようにして製造することができる。

n - ヘキシルカルバモイル- 5 - フルオロウラシル(IICFU)[三井東圧化学(開製、商品名ミフロール] 0.2 gを加えて、完全に可溶化して透明な均一溶液を得た。

別に、酸処理のゼラチン(宮坡化学側製、ゼリー強度250ブルーム)29を、1989の水に加え50℃で加温密解して1多水溶液を作成し、室温迄冷却したのち、希温酸によりPHを4.5に調整した。

t. ..

該マイクロスフェアの光紫分析値は下契の通りであり、 9.3 多のHCFUを均一に含有するものであつた。また、塩紫分析の結果、塩化ノチレンの含有は全く認められなかつた。

	C(%)	11 (%)	N (%)	F (96)
元素分析值	49.94	5 . 8 4	1,53	0.69

	5 - FU 濃度(吶/	() [: Abs (\lambda max : 270 nm)
()	7	0.135
(2)	1 4	0.28
(<u>3</u>)	2 1	0.426
Φ	2 8	0.5.5.1
(5)	3 5	0.686

試験例

HCFU粉末をPH6の生理食塩水(NaCe0.9多)に密かして「昼夜放魔後、溶出日CFUが5ーFUに分解したこの生理食塩水のUVスペクトルを測定し、吸光度と濃度が比例することを確認して下記の検視線を作成した。

これを用いて、実施例で得られたII C F U 9.3 多含有のマイクロスフェア 1 0 0 m を 5 0 ml の生理食塩水に入れ、各測定日に直接 1 ml ~ 3 ml サンプリングして直ちに U V スペクトルを測定して下表の結果を得た。

日数	(Day)	1	1	6	7	8	1 1	15	20
裕出 5-F	'U (ppm)	7.5	19	22	2 4	26	3 1	3 6	38
容出率	(%)	4	10	1 2	1.3	1 4	17	1 g	20

表より、実施例で得られたマイグロスフェ

ア微小球に製剤されたHCFU側ガン剤は、 長期間後放効果があることが確認された。

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